

2015

Analyses of ionizing radiation effects in – vitro in peripheral blood 1 lymphocytes with Raman spectroscopy

Adrian Maguire

Technological University Dublin

Isabel Vegacarrascal

Technological University Dublin

Lisa White

Technological University Dublin, lisa.white2@mydit.ie

See next page for additional authors

Follow this and additional works at: <https://arrow.tudublin.ie/radart>



Part of the [Medicine and Health Sciences Commons](#)

Recommended Citation

Maguire, A., Vegacarrascal, I. & White, L. (2015). Analyses of ionizing radiation effects in – vitro in peripheral blood 1 lymphocytes with Raman spectroscopy. *Radiation Research*, vol. 183, no. 4, pp. 407-416. doi.org/10.1667/RR13891.1

This Article is brought to you for free and open access by the Radiation and Environmental Science Centre at ARROW@TU Dublin. It has been accepted for inclusion in Articles by an authorized administrator of ARROW@TU Dublin. For more information, please contact arrow.admin@tudublin.ie, aisling.coyne@tudublin.ie.



This work is licensed under a [Creative Commons Attribution-NonCommercial-Share Alike 4.0 License](#)

Authors

Adrian Maguire, Isabel Vegacarrascal, Lisa White, B. McClean, Orla L. Howe, Fiona Lyng, and Aidan Meade

1 **Analyses of ionizing radiation effects in – vitro in peripheral blood**
2 **lymphocytes with Raman spectroscopy**

3 **A. Maguire ^{1,3}, I. Vegacarrascal ¹, L. White ^{1,2}, B. McClean⁴, O. Howe ^{1,2}, F.M.**
4 **Lyng ^{1,3}, A.D. Meade ^{1,3}**

5
6 *1. DIT Centre for Radiation and Environmental Science, Focas Research Institute, Camden*
7 *Row, Dublin 8, Ireland*

8 *2. School of Biological Sciences, Dublin Institute of Technology, Kevin Street, Dublin 8,*
9 *Ireland*

10 *3. School of Physics Dublin Institute of Technology, Kevin Street, Dublin 8, Ireland*

11 *4. Department of Medical Physics, St Luke’s Hospital (SLROC), Highfield Road, Rathgar,*
12 *Dublin 6, Ireland*

13
14 *Corresponding Author:*
15 *Aidan.Meade@dit.ie*

43 **Analyses of ionizing radiation effects in – vitro in peripheral blood**
44 **lymphocytes with Raman spectroscopy**

45 **A. Maguire^{1,3}, I. Vegacarrascal¹, L. White^{1,2}, B. McClean⁴, O. Howe^{1,2}, F.M.**
46 **Lyng^{1,3}, A.D. Meade^{1,3}**

47
48 The use of Raman spectroscopy to measure the biochemical profile of cells and tissue in health
49 and disease may be a possible solution to many diagnostic problems in the clinical setting.
50 Although its application has been extensive in identifying changes in the biochemical profiles of
51 cancerous cells and tissue, its application for analysing changes to the cellular environment by
52 external factors such as ionizing radiation has been less extensive. In tandem with this, the
53 biological impact of low doses of ionizing radiation remains poorly understood. Extensive studies
54 have been performed on the radiobiological effects associated with doses above 0.1Gy, and are
55 well characterized, but current studies of low dose exposure to ionizing radiation reveal complex
56 and highly variable responses to low dose exposures.

57 The current study demonstrates, for the first time, the capability of Raman spectroscopy to detect
58 radiation-induced damage responses in isolated lymphocytes from donors irradiated to doses of
59 0.05 Gy and 0.5 Gy. Lymphocytes were isolated from peripheral blood in a cohort of volunteers,
60 were cultured ex-vivo, and then irradiated. Within 1 hour after irradiation spectral effects were
61 observed with Raman micro-spectroscopy and Principal Component Analysis - Linear
62 Discriminant Analysis (PCA-LDA) at both doses relative to the sham-irradiated 0Gy control.
63 Cellular DNA damage was confirmed using parallel γ -H2AX fluorescence measurements on the
64 extracted lymphocytes per donor and per dose. DNA damage measurements exhibited inter-
65 individual variability between both donors and dose, which matched that seen in the spectral
66 variability in the lymphocyte cohort. Further evidence of links between spectral features and
67 DNA damage were also observed, and may potentially allow non-invasive insight into the DNA
68 remodeling after exposure to ionizing radiation.

69

70 1. Introduction

71 The mechanisms affecting high dose cell survival (at doses above ~0.1Gy) have been studied
72 extensively and are relatively well understood for a wide range of cell lines (1). The mechanisms
73 affecting low dose cell survival (at doses below ~0.1Gy) phenomena, such as low dose hyper-
74 radiosensitivity and increased radioresistance are yet to be fully understood (2). Studies have
75 shown that a region of hyper radiosensitivity (HRS) in the dose region from 0-0.3Gy, followed by
76 a region of increased radioresistance (IRR) in the region 0.3-0.6Gy (2), exists in many but not all
77 cell types (3), including peripheral blood lymphocytes (4).

78 Some suggest that this transition period is due to the activation of DNA repair systems such as the
79 activation of the ataxia telangiectaisa-mutated (ATM) gene for the recruitment of further repair
80 proteins such as the MRN complex (RAD50, MRE11 and NBS1) , which is responsible for the
81 activation of down-stream pathways (5). While there are a myriad of lesion types that can occur
82 following ionizing radiation, double strand breaks (DSBs) can be the most lethal and mutagenic if
83 not repaired properly (6). Defects in repair pathways of DSBs can result in severe responses to
84 radiotherapy or mis-diagnosis of exposure in dosimetry estimates. Histone H2AX is a molecule
85 that is recruited to the site of DSBs. ATM phosphorylates H2AX to form γ -H2AX which is then
86 used to recruit further repair molecules to the site of DSBs (7). If the ATM gene is defective then
87 this process cannot occur through the action of ATM and other less proficient pathways may be
88 activated. The measurement of phosphorylation of H2AX to γ -H2AX has been used as a method
89 of assessing DNA damage and repair. The use of the γ -H2AX assay has been demonstrated as a
90 technique that may be used for retrospective personal biodosimetry, however considerable inter-
91 individual variation in baseline levels of γ -H2AX fluorescence is problematic with this assay (9).
92 Other approaches may therefore be necessary to allow retrospective dosimetry using direct
93 biological measurements on exposed individuals.

94

95 Vibrational spectroscopy, both FTIR and Raman spectroscopy, has become a useful tool for
96 providing a complete biochemical profile of cellular contents, including nucleic acid, proteins,

97 lipids and fatty acids. Both FTIR and Raman spectroscopy have been shown to be useful for the
98 diagnosis of diseased and healthy cells based on their biochemical profiles (10–12) and while
99 extensive efforts have been made to standardize these techniques Raman spectroscopy has yet to
100 reach the clinic as a method of diagnosis. Although much emphasis has been focused on disease
101 diagnosis, Raman spectroscopy has been shown to have potential in the analysis of
102 radiobiological effects at high ionizing radiation doses in prostate tumor cell lines (13). The
103 spectral response following high doses of ionizing radiation in (13) showed changes in spectral
104 intensities of the bands associated with the O-P-O vibration of the DNA back bone at $\sim 810\text{cm}^{-1}$,
105 nucleic acid bases (U,T,C,G and A, from DNA and RNA) at 784, 1486 and 1577cm^{-1} , and several
106 bands associated with vibrations from lipids and proteins (C-C,C-N vibrations at 936 and
107 1127cm^{-1}) that allowed for discrimination between sham irradiated and irradiated cells at 24
108 hours following ionizing radiation. In addition, FTIR spectra of irradiated human skin cells have
109 demonstrated dose-dependent spectral changes that have been used for biodosimetry at both low
110 ($<0.1\text{Gy}$) and high ($>0.1\text{Gy}$) doses (14). In this study the authors show that difference in
111 absorbance spectra occur at bands associated with various vibrations arising from DNA, RNA and
112 carbohydrates (overlapping vibrations from C-O at 1200 and 1030cm^{-1} and O-H vibrations at
113 1290 and 1030) along with other characteristic vibrations from nucleic acids (U at 996cm^{-1} and
114 PO_4^- at 965cm^{-1}).

115

116 The present study demonstrates for the first time the ability of Raman spectroscopy to detect low
117 dose ionizing radiation effects in lymphocytes derived from a cohort of healthy donors.
118 Discrimination of radiation damage through the use of spectral profile changes is shown to be
119 possible at γ -radiation doses of 0.05Gy and 0.5Gy, which straddle the inflection in the cell
120 survival curve in the low dose region. Changes in spectral profiles of individuals were found to be
121 highly variable, making it difficult to create a model capable of predicting individual response to
122 low dose ionizing radiation for its use in low dose dosimetry.

123 2. Materials and methods

124 **Ethical approval**

125 Ethics approval was awarded by the Dublin Institute of Technology ethics committee (2012) for the
126 collection of blood donations from volunteers at the Institute for the purposes of this study.
127 Volunteers consisted of both male and female donors within the age range of 21 to 56, and contained
128 both smokers and non-smokers.

129 **Peripheral blood lymphocyte isolation**

130 A total of 20ml of fresh whole blood was drawn into lithium heparin tubes after obtaining informed
131 consent from each of the donors. Peripheral blood mononuclear cells (PBMC) were isolated within 4h
132 of sample collection. A total of 6 ml of Dulbecco's modified phosphate buffered saline (DPBS)
133 (Sigma) was added to 6 ml of heparinised blood, mixed by gentle inversion and overlaid over 15 ml
134 of Histopaque. Samples were then centrifuged at 400g for 30 min at room temperature. The PBMC
135 layer was removed and washed three times. Finally, cells were centrifuged at 250g for 5 minutes at
136 room temperature. The cell pellet was then resuspended in 3 ml of full media (RPMI+12.5 %(v/v)
137 FBS + 2 mM-L-glutamine (Sigma)) supplemented with 2.5% (v/v) phytohaemagglutinin (PAA
138 Laboratories). One ml of cell suspension was transferred to a T25 flask containing 4ml of full media.
139 A total of 3 flasks were prepared for each donor and they were incubated for 72 hours at 37°C, 5%
140 CO₂ to allow separation of lymphocytes and monocytes by plastic adherence.

141 **Cell Irradiation and slide preparation**

142 A total of 5ml of cell suspension was placed in T25 flasks for irradiation. The flasks were either sham
143 irradiated (0Gy) or irradiated (0.05Gy and 0.5Gy) 17 hours after plating using a cobalt 60 gamma ray
144 teletherapy source at St. Luke's hospital, Dublin. The dose rate was approximately 1.5 Gy/min during
145 these experiments and was determined from a decay corrected measurement of the in-beam axial dose
146 at an 80cm source to chamber distance (measured using a secondary standard ionization chamber
147 within a water equivalent phantom). The dose settings that were used and the actual dose delivered,
148 with their respective uncertainties, were 0.05Gy (0.058Gy ± 17%) and 0.5Gy (0.511Gy ± 2%). The

149 actual dose that was delivered at the time of irradiation was determined from the axial dose, corrected
150 for scatter and grid factors, the additional time that the sample was exposed to radiation ((with an
151 accuracy of ± 0.005 min) during the extension and recession of the source from the within the cobalt
152 unit), and source to sample distance (191.5cm for 0.05Gy and 100cm for 0.5Gy). The samples were
153 then placed in an incubator at 37°C for 60 mins at which time, cells were fixed using 2%
154 paraformaldehyde in phosphate-buffered saline. From the suspension, 40 μ l was drop cast onto
155 calcium fluoride (CaF₂) slides. The slides were then washed in deionised H₂O and the samples were
156 allowed to dry for Raman spectroscopic measurements.

157 **Raman Spectroscopy**

158 Raman spectroscopy was performed using a Horiba Jobin Yvon Labram HR800 UV system, equipped
159 with a 660nm solid-state diode laser delivering 100mW of power to the sample. Spectra were
160 acquired for each of 20 different donors over a period of 6 months. All samples (sham irradiated cells
161 (0Gy) and irradiated samples (0.05Gy and 0.5Gy) from each individual were recorded on the same
162 day, together with a spectrum of 1,4-Bis (2-methylstyryl) benzene and NIST SRM 2245 for
163 calibration purposes. Multiple calibration spectra were recorded before recording a sequential group
164 of cellular spectra. Spectra were recorded from 30-40 cells per dose and time point and from each of
165 the independent donors. The cells were ~ 8 -12 μ m in size and each spectrum was recorded from
166 individual cells using a 4x4 μ m raster scan of the cell including both signal from its nucleus and
167 cytoplasm. Spectra were recorded with a 20 second integration time and averaged across three
168 integrations per spectrum. Spectra were recorded using a diffraction grating ruled with 300 lines/mm
169 giving a spectral resolution of ~ 2.1 cm⁻¹. The confocal hole was set to 150 μ m with the grating centered
170 at 1350cm⁻¹. All spectra were recorded within two weeks of slide preparation. Slides were stored in a
171 desiccator until measurement.

172 **Raman spectral post processing**

173 All post processing was performed using Matlab version 7.9.0 (R2009b; Mathworks, USA) using the
174 PLS-Toolbox version 6.51 (Eigenvector Research Inc.) and in-house algorithms. The spectra were

175 wavenumber aligned using the calibration spectrum of 1, 4-Bis (2-methylstyryl) benzene through the
176 fitting of a polynomial to the relative positions of peaks in the calibration spectrum versus those in a
177 common reference spectrum of the substance. This results in a spectral misalignment of $<0.1 \text{ cm}^{-1}$
178 through day-to-day variation. Spectral intensity calibration was also performed using a reference
179 spectrum of standard reference material SRM2245 (NIST). Baseline correction was performed using a
180 nodal point baseline correction using the minimum amount of points possible to ensure minimal
181 alteration of the spectra. Spectra were then lightly smoothed using a Savitsky Golay filter (5th order,
182 15 point window). Substrate contributions from the CaF_2 slide were also subtracted from the cellular
183 spectra. All spectra were subsequently vector normalised before analysis.

184 **Principal component analysis-Linear discriminant analysis and statistical** 185 **analysis**

186 Multivariate data classification approaches including Principal Component Analysis (PCA) with
187 Linear Discriminant Analysis (LDA) have been used to identify features that can classify spectra in an
188 unsupervised manner (10,15). Cellular Raman spectra consist of many overlapping regions from
189 different constituents. PCA removes this redundancy while LDA attempts to discriminate between
190 conditions using the previously determined principal components. In this study PCA-LDA is used to
191 discriminate between sham irradiated and irradiated donor lymphocytes. All classifications in this
192 study were performed using a Leave-One-Out-Cross validation (LOOCV) approach and confusion
193 matrices, sensitivities and specificities were calculated on the basis of LOOCV.

194 Statistical testing of each wavenumber was performed across the spectrum, to identify regions of the
195 spectrum that the irradiated spectra varied significantly from the sham irradiated spectra. Significance
196 testing was performed using a two tailed t-test independently on each wavenumber. Each irradiated
197 samples wavenumber was found to be significantly different from the sham if the significance level
198 was found to be $p < 0.05$.

199 γ -H2AX assay

200 Cells were fixed at 1 hour after irradiation and frozen at -20°C. They were later permeabilised in 200-
201 1000 μ l of 0.25% (v/v) Triton X-100 in PBS and incubated for 5 minutes at room temperature.
202 Permeabilisation solution was then removed and the cells were resuspended in 200 μ l of blocking
203 solution (PBS containing 2% (w/v) BSA) and incubated for 30 minutes at room temperature.
204 Blocking solution was removed and the cells were resuspended in 150 μ l of primary antibody solution
205 (Anti-phospho-histone H2AX, diluted 1:500 in blocking solution, Millipore) and incubated for a
206 further 2 hours at room temperature. Washing was performed three times in 500 μ l of PBS and 150 μ l
207 of secondary antibody solution (Alexa Fluor 488, diluted 1:200 in blocking solution, Invitrogen) was
208 then added. The cells were incubated at room temperature for 1 hour in the dark and washing was
209 performed in 500 μ l PBS three times. Fluorescence was analysed using a BD Accuri C6 flow
210 cytometer. The mean fluorescence signal intensity due to green Alexa Fluor 488 dye was measured. A
211 minimum of 10,000 events per sample were recorded, debris and cell aggregates were removed from
212 the analysis using forward (FSC) and side scatter (SSC) characteristics. Significance testing was
213 performed between sham irradiated and irradiated γ -H2AX measurements using a two tailed paired t-
214 test.

215

216 **3. Results**

217 **Raman spectroscopic analysis of sham irradiated and irradiated donor** 218 **lymphocytes.**

219 Figure 1 A shows the mean spectra from sham irradiated (0Gy) lymphocytes from 20 donors along
220 with the pure spectra of DNA, RNA, phosphatidyl-inositol and actin. The spectral profiles of donor
221 lymphocytes in this study are consistent with that observed in previous studies by (16–19), with bands
222 observed at 770-790 cm^{-1} arising from vibrations associated with the DNA double helix, 1000-1003
223 cm^{-1} occurring as a result of the vibrations of phenylalanine (20) and bands occurring in the regions

224 1250-1350, 1400-1450 and 1500-1700 cm^{-1} (Amide I,II and III bands) associated with proteins, lipids
225 and nucleic acids (21,22). The dotted dashed lines in the plot are to highlight typical spectral bands
226 associated with biological species and band assignments are provided in table 1. Figure 1 B (top)
227 shows the difference spectrum of sham irradiated and irradiated (0.05Gy) cells and the difference
228 spectrum of sham irradiated and irradiated (0.5Gy) (bottom) cells fixed at 1 hour following ionizing
229 radiation. Samples were fixed at one hour following ionizing radiation in order to correlate the initial
230 DNA damage sensing measured by the change in Raman spectral profiles, to the DNA damage
231 sensing measured by the γ -H2AX assay. Analysis of later time points would result in measurement of
232 residual damage rather than initial DNA damage sensing (measured by γ -H2AX), where Raman
233 spectroscopy may also measure changes in spectral profiles due to pathways downstream of initial
234 sensing, such as cell cycle arrest, senescence and apoptosis. These cellular processes will result in
235 changes in spectral profiles due to the up or down regulation of repair proteins and proteins associated
236 with the other DNA damage responses in addition to the changes in spectral profiles due to the initial
237 DNA damage response. The spectra of pure DNA and actin are plotted above and below the
238 difference spectrum to highlight some of the origins of the change in spectral profiles of donor
239 lymphocytes following ionizing radiation. The lightly shaded regions of Figure 1 B represent regions
240 of the spectrum where irradiated samples had significantly higher intensities than that of the sham.
241 The darker shaded regions represent regions of the spectrum where irradiated samples had
242 significantly lower intensities than that of the sham. A similar change is observed in both doses with
243 the exception of the band at 1650cm^{-1} in the Amide I region, which is associated with C=C stretching
244 in protein and lipid (38). Increases in the regions $610\text{-}620\text{ cm}^{-1}$ (associated with C-C twisting of
245 aromatic ring structure (20,23)), $635\text{-}640\text{ cm}^{-1}$ (C-S stretching and C-C twisting of proteins (20)),
246 $715\text{-}825\text{ cm}^{-1}$ (C-N membrane of phospholipids and phosphatidylcholine, A, T, U and C ring
247 breathing and O-P-O DNA backbone stretching (22,24-27)), $845\text{-}850\text{ cm}^{-1}$ (Monosacchrides,
248 polysacchrides and glucose (22,28)), $927\text{-}955\text{ cm}^{-1}$ (C-C stretching of amino acids proline and valine
249 (29)), $1320\text{-}1340\text{ cm}^{-1}$ (G (DNA/RNA) and CH deformation (27)), $1565\text{-}1650\text{ cm}^{-1}$ (G and A nucleic
250 acids and C=C bending (29,30)) and $1750\text{-}1800\text{ cm}^{-1}$ (C=O and C=C in lipids and fatty acids (24,31))

251 were observed following ionizing radiation. Decreases in the regions 675-700 cm^{-1} (Ring breathing of
252 DNA base G (20)), 1005-1020 cm^{-1} ((significantly less after 0.5Gy only) Phenylalanine and
253 stretching of C-O of ribose (27,32)), 1085-1090 cm^{-1} (C-C vibration of acyl backbone in lipids and
254 PO_2 stretching (21,24,33)), 1100-1125 cm^{-1} (Amide III (21)), 1255-1275 cm^{-1} (A, T, C and G nucleic
255 acids, Amide III (20,26,34,35)), 1420-1425 cm^{-1} (G, A of nucleic acids and CH deformation (27)) and
256 1450-1525 cm^{-1} (CH_2 bending, C=N stretching of lipids (36,37)) were observed following ionizing
257 radiation. Although there is a change in the mean of the intensities of these bands, the distributions
258 overlap considerably across the cohort of donors.

259 Figure 2 A shows the difference spectra of control versus 0.05Gy in a total of 5 donors. In all cases
260 there is a change in spectral profiles in the region 700-830 cm^{-1} associated with nucleic acids and the
261 phosphate backbone of DNA, the region 1070-1115 cm^{-1} associated with C-C stretching of lipids and
262 fatty acids, the band at 1094 cm^{-1} associated with the O-P-O stretching vibration of the DNA
263 backbone, the region from 1550-1600 cm^{-1} associated with amide II band, tryptophan, guanine and
264 adenine, and the region 1640-1730 cm^{-1} associated with the amide I, proteins, lipids and fatty acids.
265 Although the variation consistently occurs in these regions the changes in spectral profile after
266 0.05Gy irradiation are inconsistent, with some donors having increases in band intensities in these
267 regions and others having decreases in band intensities. Aside from these regions there is a large
268 variation in the changes in spectral profiles following ionizing radiation throughout the rest of the
269 spectrum, with large variation occurring in the region 1150-1520 cm^{-1} which is associated with
270 nucleic acids, proteins, lipids and fatty acids. Similar variation is observed in the spectral changes
271 following 0.5Gy of ionizing radiation. Figure 2 B shows the difference spectra of 0.5Gy and 0Gy for a
272 different 5 donors. Again variations are consistently observed in the regions 700-830 cm^{-1} , 1070-
273 1115 cm^{-1} and 1550-1600 cm^{-1} , but the change in spectral profile in these regions is inconsistent from
274 donor to donor. This matches that of the inter-individual variability in the baseline levels of γ -H2AX
275 which are discussed under the *γ -H2AX fluorescence measurements* section.

276

277 **Classification of donor cohort by dose.**

278 PCA-LDA was performed on each donor's spectra independently and classifications were performed
279 on control spectra against 0.05Gy spectra, control spectra against 0.5Gy spectra and 0.05Gy against
280 0.5Gy spectra. PCA-LDA was performed using three principal components which were selected to
281 maximize the sensitivity and specificity of each classification and such that they explained ~80% of
282 the total variance in the spectra. The performance of the classifiers was calculated using leave-one-
283 out-cross-validation (LOOCV). Figure 3 A shows the scatter plot of the PCA-LDA classification of
284 sham irradiated and irradiated cells (0.05Gy) spectra from a single donor (Donor number 5). Principal
285 component loadings are not shown due to the large inter-individual variability in the spectral features
286 associated with the classification, however in all instances the principal components for each
287 individual showed a high correlation to that of their difference spectra shown in Figure 2. The
288 Matthews correlation coefficient (MCC) of the classification in Figure 3 A, was 0.79 with a
289 sensitivity of 0.81 and a specificity of 1. MCC is used here to give a weighted combination of
290 sensitivity and specificity, a value of +1 results in a classifier that predicts all instances correctly, a
291 value of 0 results in a classifier that has a 50% chance of classifying any instance correctly and a
292 value of -1 indicates that the classifier classifies each instance incorrectly. Figure 3 B shows the
293 scatter plot of the PCA-LDA classification of sham irradiated and irradiated cells (0.5Gy) from the
294 same donor. The Matthews correlation coefficient of this classification was 0.93 with a sensitivity of
295 0.97 and a specificity of 0.97. In Figure 3 A the second principal component, which explains 22% of
296 the total variance, is the principal component primarily responsible for the classification as the
297 separation in the classes occurs along its axis. In Figure 3 the classification is due to a combination of
298 principal components two and three mainly. The first principal component in both classifications was
299 found to be almost identical and contributes very little to the performance of the classification
300 (Principal component not shown). This principal component may arise from the variability in the
301 spectra which arises from the inherent variability in the cell cycle distribution within the cell
302 population, as the features in this component were found to be consistent with those observed by
303 Matthews et al in (40). In both studies positive peaks in the first principal component occurred at

304 ~670cm⁻¹ (Guanine and thymine), 719cm⁻¹ (choline), 728cm⁻¹ (Adenine), 1100cm⁻¹ (Phosphate
305 backbone of DNA/RNA), ~1245cm⁻¹ (Amide III β), 1450-1480cm⁻¹ (Adenine, Guanine), 1575cm⁻¹
306 (Adenine, Guanine) and 1680cm⁻¹(Amide I β). Negative peaks were observed in the principal
307 components of both studies at ~700cm⁻¹ (cholesterol),~ 1130cm⁻¹ (C-C from lipids and C-N from
308 proteins) and 1440cm⁻¹ (CH₂ deformation).

309

310 PCA-LDA classification models were created for each donors sham irradiated and irradiated cells
311 separately. A mean sensitivity and specificity of 0.88 ($\sigma = 0.1$) and 0.91 ($\sigma = 0.07$) respectively were
312 obtained for classification of spectra from the 0.05Gy samples versus the sham irradiated samples.
313 Similarly sensitivities and specificities of 0.92 ($\sigma = 0.07$) and 0.93 ($\sigma = 0.07$) respectively were seen
314 in the classification of the 0.5Gy samples versus the sham. The sensitivities and specificities for each
315 donor's classifications are listed in table 2, in order of decreasing values of sensitivity. Larger values
316 of sensitivity and specificity indicate larger changes in spectral profiles between classification
317 conditions (0Gy v 0.05Gy, 0Gy v 0.5Gy or 0.05Gy v 0.5Gy). The variation in the classification
318 sensitivities and specificities at each dose point demonstrates the variability in the changes in spectral
319 profile of lymphocytes from donor to donor after ionizing radiation, which matches that of the
320 variability of the dose response in the γ -H2AX assay. The classification rates for each individual show
321 clearly that Raman spectroscopy can detect changes in spectral profiles between sham irradiated and
322 irradiated cells at doses as low as 0.05Gy.

323

324 PCA-LDA classification was also performed using a pooled set of all on all donor spectra
325 simultaneously. Classification of sham irradiated versus 0.05Gy and sham irradiated versus 0.5Gy,
326 using a set of latent variables explaining up to 90% of the total variance of the spectra, demonstrated
327 that there was a spectral difference between sham irradiated and irradiated cells with a mean MCC of
328 0.32 and 0.41 across all donors. Classification accuracies were estimated using a leave-one-donor-out
329 cross-validation for varying numbers of latent variables to optimize the classification rate.
330 Optimisation was performed using the training (all spectra except those from a single held-back
331 donor) and testing (held-back spectra from one donor) sets of control versus 0.5Gy spectra. Both

332 training and testing sets classification performance was assessed using MCC. The training set
333 performed relatively well when 35 or more latent variables were used in the classification and resulted
334 in an $MCC > 0.3$, however no model performed well on the test set where no model achieved an MCC
335 of greater than 0.05 (data not shown). This demonstrates that although Raman spectroscopy can detect
336 changes in biochemical profiles of individual donors following ionizing radiation, classification of
337 response in individuals using data learned from a cohort of donors is difficult as demonstrated by the
338 optimization not achieving an MCC greater than 0.05.

339

340 **γ -H2AX fluorescence measurements**

341 Parallel reference measurements of DNA damage following ionizing radiation were obtained using
342 the γ -H2AX assay. A large inter-individual variation in baseline levels of γ -H2AX fluorescence was
343 observed. In this study a significant difference was observed in γ -H2AX fluorescence following
344 ionizing radiation only when samples were normalized to their own control (two tailed paired t-test).
345 Figure 4 A) shows the normalized γ -H2AX fluorescence with respect to dose. A dose response was
346 observed following ionizing radiation and 0.05Gy was found to be significantly different from the
347 control with a significance level of $p < 0.05$, while 0.5Gy was found to be significantly different from
348 the controls with a significance level of $p < 0.01$. The variation in inter-individual response to ionizing
349 radiation detected using γ -H2AX fluorescence is consistent with that of the variation observed in the
350 classification of Raman spectral data. In some donors the γ -H2AX fluorescence increases more so
351 than others following ionizing radiation; similarly the change in spectral information following
352 ionizing radiation is more prevalent in some donors than others. This is evident from the ability of the
353 classifier to distinguish between sham irradiated and irradiated cells in different donors. Higher
354 sensitivities and specificities indicate a larger change in spectral profile following ionizing radiation,
355 while lower sensitivities and specificities indicate a lack of change in the spectral profile of sham
356 irradiated and irradiated cells (see Table 2). While there is large inter individual variation in the
357 response to ionizing radiation measured by both the γ -H2AX assay and Raman spectral
358 measurements, there is an increase in the band areas that were found to be significantly different from

359 the control which matched that of the γ -H2AX assay. In both γ -H2AX and Raman spectral
360 measurements a dose response was observed. The correlation between the band areas and the γ -H2AX
361 MFI is shown in Figure 4 B).

362

363 Figure 5 A shows the frequency distribution of the γ -H2AX fluorescence measurements with dose for
364 all 20 donors. It demonstrates the frequency of which a measurement of γ -H2AX was measured
365 within a particular range of γ -H2AX MFI for all 20 donors both sham irradiated and irradiated. The
366 black curve represents the probability distribution function and the vertical line represents the mean γ -
367 H2AX fluorescence for each dose. The probability distribution function describes the likelihood of a
368 random measurement to be within a particular interval and the peak of the probability density function
369 is the interval that represents the most likely outcome of any given measurement. The distribution
370 shows an increase in γ -H2AX fluorescence following ionizing radiation as the probability distribution
371 shifts to higher γ -H2AX MFI with the frequency of low levels of γ -H2AX MFI is decreasing and the
372 frequency of higher levels of γ -H2AX MFI is increasing. Large inter-individual variability was
373 observed in the baseline levels of γ -H2AX fluorescence and can be seen from this plot as the
374 frequencies of γ -H2AX MFI span a large range in all doses and overlap between doses. Similarly to
375 the γ -H2AX fluorescence measurements, Figure 5 B shows the frequency distribution of the total area
376 of the regions of the spectrum with higher intensities than the sham in terms of dose. Although the
377 distributions overlap considerably, a positive correlation to γ -H2AX MFI was observed with the total
378 area of the regions that were significantly higher than the control (see Figure 4 B). A shift in the
379 probability distribution function towards higher band areas was observed following ionizing radiation
380 with a decrease in the frequency of lower band areas and an increase in the frequency of higher band
381 areas. The increase in area of these bands is a result of the increase in the intensities observed in the
382 bands at $720\text{-}850\text{cm}^{-1}$ associated with the vibrations occurring from the backbones and nucleic acid
383 bases of DNA and RNA and $1640\text{-}1660\text{cm}^{-1}$ associated with proteins and lipids. The changes in the
384 distribution of the total area of these bands following ionizing radiation were found to be significantly
385 different in the sham spectra versus the irradiated spectra, with a significance level of $p < 0.001$. The
386 significance testing reveals that Raman spectroscopy can detect changes in the spectroscopic finger

387 print of cells following ionizing radiation in a normal population at 1 hour after exposure to ionizing
388 radiation but as the distributions overlap considerably classification of individual responses becomes
389 more difficult.

390 **5. Discussion**

391 The use of the γ -H2AX assay for dosimetry measurements has been shown previously by (9) to have
392 high levels of inter-individual variation, while a dose response following ionizing radiation was
393 observed. In this study, high levels of inter-individual baseline variation has been observed within a
394 cohort of 20 donor lymphocytes and when samples were normalized to their controls a dose response
395 was observed and was found to be statistically significantly. Raman spectroscopy has been shown to
396 be capable of detecting changes in spectral profiles of irradiated lymphocytes compared to sham
397 irradiated lymphocytes at doses as low as 0.05Gy. Unlike the γ -H2AX assay, however, the detection
398 of changes following ionizing radiation are not limited to a single molecule in Raman spectroscopy.
399 Instead Raman spectroscopy provides a cellular biochemical fingerprint containing signatures of
400 nucleic acids, proteins, lipids and fatty acids. The changes in spectral profiles are highly variable from
401 individual to individual matching that of the γ -H2AX inter-individual variability. Large variability in
402 the change in spectral bands associated with nucleic acids (in the region of 720-850 cm^{-1}), proteins and
403 lipids (1200-1350 cm^{-1}) was observed from individual to individual. The variability in the change in
404 these bands may be due to the variation in age, gender, lifestyle, eating habits and genetic
405 predisposition. PCA-LDA showed poor classification performance when all donors were classified
406 and tested simultaneously, using a leave-one-donor-out cross-validation. Significance testing revealed
407 that there were several regions of the spectrum where the intensities of the spectra of irradiated cells
408 were either significantly higher or lower than that of the control cells. Similarly to the variation
409 observed in the baseline levels of the γ -H2AX assay the areas under these regions overlap
410 considerably between doses making uni-variate classification for the purpose of dosimetry difficult.
411 However, changes to distribution of the area under these regions may provide an alternative method
412 of dosimetry.

413 **Analysis of intensity changes in spectral data with dose**

414 The changes in the intensities of the regions that were observed to differ from the controls following
415 ionizing radiation indicate variation in the spectral information from nucleic acids, lipids and proteins.
416 Increases were observed in the band intensities associated with DNA, RNA, lipids and proteins. This
417 suggests that Raman spectroscopy measures an increase in the level of RNA (band at 750-825 cm^{-1})
418 and thus an increase in transcription and gene expression following ionizing radiation. This is in
419 contrast to that of the γ -H2AX measurements which measures only the phosphorylation of H2AX as a
420 result of ATM activation. The changes in spectral profiles also contain signatures of damage and
421 cellular responses from not only double strand breaks but single strand breaks and other lesion types
422 as the variation in vibrational modes are not limited to alterations in the O-P-O stretching of the DNA
423 backbone. Changes were observed in regions of the spectrum which have been associated with double
424 strand breaks of the DNA (41). Bands around 1110 cm^{-1} , 1160 cm^{-1} and 1190 cm^{-1} were significantly
425 altered after irradiation relative to the sham and are as a result of cleavage of the DNA phosphate
426 backbone at either at the 3' end of one DNA strand and the 5' prime end the other strand or at the 5'
427 end on both strands of the DNA. Some of these changes in spectral profiles are consistent with those
428 observed elsewhere (42) after high doses of ionizing radiation.

429

430 For a more robust analysis, there is need for larger studies with Raman spectroscopy coupled with
431 parallel reference measurements of DNA damage, repair, cell viability and other high content data.
432 Inclusion of additional data on the individual such as age, gender, ethnicity, lifestyle and health status
433 in modeling of biological data at low doses might also account for the high level of inter-individual
434 variability at low doses. These approaches may in the future provide further insight into the spectral
435 changes following ionizing radiation and will aid in the development of multivariate models.

436

437 **6. Conclusion**

438 The present study demonstrates the capability of Raman spectroscopy to detect changes in spectral
439 profiles following low dose ionizing radiation in a cohort of 20 donor lymphocytes as little as 1 hour
440 after exposure to ionizing radiation. This is the first report where Raman spectroscopy has been
441 shown to be capable of classifying control samples against irradiated samples with doses as low as
442 0.05Gy in individuals.

443 **7. Acknowledgments**

444 The authors would like to express sincere thanks to Laura Shields, Chris Walker and Padraic Crean
445 (SLROC) for their generous co-operation. This work was financially supported by the EU FP7
446 Network of Excellence DoReMi (Grant Number 249689).

447 **8. References**

- 448 1. Deschavanne PJ, Fertil B. A Review of Human Cell Radiosensitivity in Vitro. *Int J Radiat*
449 *Oncol *Biology*Physics*. 1996;34(1):251–66.
- 450 2. Marples B, Collis SJ. Low-dose hyper-radiosensitivity: past, present, and future. *Int J Radiat*
451 *Oncol Biol Phys*. 2008 Apr 1;70(5):1310–8.
- 452 3. Mothersill C, Seymoura CB, Joiner MC. Low-Dose between Relationship Hypersensitivity
453 and the Bystander Effect. *Radiat Res*. 2002;157(5):526–32.
- 454 4. Nasonova E a, Shmakova NL, Komova O V, Mel'nikova L a, Fadeeva T a, Krasavin E a, et al.
455 Cytogenetic effects of low-dose radiation with different LET in human peripheral blood
456 lymphocytes. *Radiat Environ Biophys*. 2006 Nov;45(4):307–12.
- 457 5. Hoeijmakers JHJ. Genome maintenance mechanisms for preventing cancer. 2001;366–74.
- 458 6. Jeggo P, Lavin MF. Cellular radiosensitivity: how much better do we understand it? *Int J*
459 *Radiat Biol*. 2009 Dec;85(12):1061–81.

- 460 7. Burma S, Chen BP, Murphy M, Kurimasa a, Chen DJ. ATM phosphorylates histone H2AX in
461 response to DNA double-strand breaks. *J Biol Chem*. 2001 Nov 9;276(45):42462–7.
- 462 8. Kinner A, Wu W, Staudt C, Iliakis G. Gamma-H2AX in recognition and signaling of DNA
463 double-strand breaks in the context of chromatin. *Nucleic Acids Res*. 2008 Oct;36(17):5678–
464 94.
- 465 9. Horn S, Barnard S, Brady D, Prise KM, Rothkamm K. Combined analysis of gamma-
466 H2AX/53BP1 foci and caspase activation in lymphocyte subsets detects recent and more
467 remote radiation exposures. *Radiat Res*. 2013 Dec;180(6):603–9.
- 468 10. Crow P, Barrass B, Kendall C, Hart-Prieto M, Wright M, Persad R, et al. The use of Raman
469 spectroscopy to differentiate between different prostatic adenocarcinoma cell lines. *Br J*
470 *Cancer*. 2005 Jun 20;92(12):2166–70.
- 471 11. Krafft C, Steiner G, Beleites C, Salzer R. Disease recognition by infrared and Raman
472 spectroscopy. *J Biophotonics*. 2009 Feb;2(1-2):13–28.
- 473 12. Lyng FM, Faoláin EO, Conroy J, Meade a D, Knief P, Duffy B, et al. Vibrational spectroscopy
474 for cervical cancer pathology, from biochemical analysis to diagnostic tool. *Exp Mol Pathol*.
475 2007 Apr;82(2):121–9.
- 476 13. Matthews Q, Jirasek a, Lum JJ, Brolo a G. Biochemical signatures of in vitro radiation
477 response in human lung, breast and prostate tumour cells observed with Raman spectroscopy.
478 *Phys Med Biol*. 2011 Nov 7;56(21):6839–55.
- 479 14. Meade AD, Clarke C, Byrne HJ, Lyng FM. Fourier transform infrared microspectroscopy and
480 multivariate methods for radiobiological dosimetry. *Radiat Res*. 2010 Feb;173(2):225–37.
- 481 15. Das K, Stone N, Kendall C, Fowler C, Christie-Brown J. Raman spectroscopy of parathyroid
482 tissue pathology. *Lasers Med Sci*. 2006 Dec;21(4):192–7.
- 483 16. Chan JW, Taylor DS, Zwerdling T, Lane SM, Ihara K, Huser T. Micro-Raman spectroscopy
484 detects individual neoplastic and normal hematopoietic cells. *Biophys J*. 2006 Jan
485 15;90(2):648–56.

- 486 17. Pully V V., Lenferink a. TM, Otto C. Time-lapse Raman imaging of single live lymphocytes. J
487 Raman Spectrosc. 2011 Feb 15;42(2):167–73.
- 488 18. Mannie MD, McConnell TJ, Xie C, Li Y-Q. Activation-dependent phases of T cells
489 distinguished by use of optical tweezers and near infrared Raman spectroscopy. J Immunol
490 Methods. 2005 Feb;297(1-2):53–60.
- 491 19. Takai Y, Masuko T, Takeuchi H. Lipid structure of cytotoxic granules in living human killer T
492 lymphocytes studied by Raman microspectroscopy. Biochim Biophys Acta. 1997 Apr
493 17;1335(1-2):199–208.
- 494 20. Chan JW, Taylor DS, Zwerdling T, Lane SM, Ihara K, Huser T. Micro-Raman spectroscopy
495 detects individual neoplastic and normal hematopoietic cells. Biophys J. Elsevier; 2006 Jan
496 15;90(2):648–56.
- 497 21. Lakshmi R., Kartha VB, Murali Krishna C, R Solomon JG, Ullas G, Uma Devi P. Tissue
498 Raman spectroscopy for the study of radiation damage: brain irradiation of mice. Radiat Res.
499 2002 Feb;157(2):175–82.
- 500 22. Krafft C, Neudert L, Simat T, Salzer R. Near infrared Raman spectra of human brain lipids.
501 Spectrochim Acta A Mol Biomol Spectrosc. 2005 May;61(7):1529–35.
- 502 23. Ó Faoláin E, Hunter MB, Byrne JM, Kelehan P, McNamara M, Byrne HJ, et al. A study
503 examining the effects of tissue processing on human tissue sections using vibrational
504 spectroscopy. Vib Spectrosc. 2005 Jul;38(1-2):121–7.
- 505 24. Stone N, Kendall C, Smith J, Crow P, Barr H. Raman spectroscopy for identification of
506 epithelial cancers. Faraday Discuss. 2004;126:141.
- 507 25. Farquharson S, Shende C, Inscore FE, Maksymiuk P, Gift A. Analysis of 5-fluorouracil in
508 saliva using surface-enhanced Raman spectroscopy. J Raman Spectrosc. 2005 Mar;36(3):208–
509 12.
- 510 26. Ruiz-Chica AJ, Medina MA, Sanchez-Jimenez F, Ramirez FJ. Characterization by Raman
511 spectroscopy of conformational changes on guanine- cytosine and adenine-thymine

- 512 oligonucleotides induced by aminoxy analogues of spermidine. *J Raman Spectrosc.*
513 2004;35:93–100.
- 514 27. Notingher I, Green C, Dyer C, Perkins E, Hopkins N, Lindsay C, et al. Discrimination between
515 ricin and sulphur mustard toxicity in vitro using Raman spectroscopy. *J R Soc Interface.* 2004
516 Nov 22;1(1):79–90.
- 517 28. Gniadecka M, Wulf HC, Mortensen NN, Nielsen OF, Christensen DH. Diagnosis of basal cell
518 carcinoma by Raman spectroscopy., 28: 125–129. *J Raman Spectrosc.* 1997;28:125–9.
- 519 29. Lau DP, Huang Z, Lui H, Man CS, Berean K, Morrison MD, et al. Raman spectroscopy for
520 optical diagnosis in normal and cancerous tissue of the nasopharynx-preliminary findings.
521 *Lasers Surg Med.* 2003 Jan;32(3):210–4.
- 522 30. Shaw RA, Mantsch HH. Vibrational biospectroscopy: from plants to animals to humans. A
523 historical perspective. *J Mol Struct.* 1999 May;480-481:1–13.
- 524 31. Malini R, Venkatakrishna K, Kurien J, Pai KM, Rao L, Kartha VB, et al. Discrimination of
525 Normal , Inflammatory , Premalignant , and Malignant Oral Tissue: A Raman Spectroscopy
526 Study. 2006;81:179–93.
- 527 32. Seballos L, Zhang JZ, Sutphen R. Surface-enhanced Raman scattering detection of
528 lysophosphatidic acid. *Anal Bioanal Chem.* 2005 Nov;383(5):763–7.
- 529 33. Cheng W-T, Liu M-T, Liu H-N, Lin S-Y. Micro-Raman spectroscopy used to identify and
530 grade human skin pilomatrixoma. *Microsc Res Tech.* 2005 Oct;68(2):75–9.
- 531 34. Dukor RK. Biomedical Applications in Handbook of Vibrational Spectroscopy. 2002.
- 532 35. Kolijenic S, Scut TB, Vincent A, Kros JM, Puppels GJ. Detection of Meningioma in Dura
533 Mater by Raman Spectroscopy. 2005;77(24):7958–65.
- 534 36. Kaminaka S, Ito T, Yamazaki H, Kohda E, Hamaguchi H. Near-infrared multichannel Raman
535 spectroscopy toward real-time in vivo cancer diagnosis. *J Raman Spectrosc.* 2002
536 Jul;33(7):498–502.

- 537 37. Shetty G, Kendall C, Shepherd N, Stone N, Barr H. Raman spectroscopy: elucidation of
538 biochemical changes in carcinogenesis of oesophagus. *Br J Cancer*. 2006 May
539 22;94(10):1460–4.
- 540 38. Movasaghi Z, Rehman S, Rehman IU. Raman Spectroscopy of Biological Tissues. *Appl*
541 *Spectrosc Rev*. 2007 Sep;42(5):493–541.
- 542 39. Binoy J, Abraham JP, Joe IH, Jayakumar VS, Pettit GR, Nielsen OF. NIR-FT Raman and FT-
543 IR spectral studies and ab initio calculations of the anti-cancer drug combretastatin-A4. *J*
544 *Raman Spectrosc*. 2004 Nov;35(11):939–46.
- 545 40. Matthews Q, Jirasek A, Lum J, Duan X, Brolo AG. Variability in Raman spectra of single
546 human tumor cells cultured in vitro: correlation with cell cycle and culture confluency. *Appl*
547 *Spectrosc*. 2010 Aug;64(8):871–87.
- 548 41. Lipiec E, Sekine R, Bielecki J, Kwiatek WM, Wood BR. Molecular characterization of DNA
549 double strand breaks with tip-enhanced Raman scattering. *Angew Chem Int Ed Engl*. 2014 Jan
550 3;53(1):169–72.
- 551 42. Matthews Q, Brolo A, Lum J, Duan X, Jirasek a. Raman spectroscopy of single human tumour
552 cells exposed to ionizing radiation in vitro. *Phys Med Biol*. 2011 Jan 7;56(1):19–38.

553

554 9. Table of figures

555 Figure 1: A) The mean of all 20 donors sham-irradiated spectra along with spectra of DNA,
556 RNA, phosphatidyl-inositol (a typical phospho-lipid) and actin (a typical protein). Guides are
557 included to link some modes of vibration in component spectra to modes of vibration in
558 lymphocytes. Pure DNA, RNA, phosphatidyl-inositol and actin were purchased from Sigma-
559 Aldrich and used without further preparation. 23

560 Figure 2: A) Difference spectra of 0.05Gy and 0Gy for 5 donor's spectra and B) Difference
561 spectra of 0.5Gy and 0Gy for 5 donor's spectra. 25

562 Figure 3: The scatter plots of PCA scores of 0Gy and 0.05Gy (A), and 0Gy and 0.5Gy (B)
563 spectra of a single healthy donor and for the first three principal components. The grey line
564 represents the plane of discrimination determined by LDA. 26

565 Figure 4: A) Normalised γ -H2AX fluorescence with respect to dose for all donors.
566 Significance testing was performed using a two tailed paired t-test. B) Normalised γ -H2AX
567 MFI with respect to the total area of the bands of the spectrum that were found to be
568 significantly higher than the sham. Error bars indicate the standard error. 27

569 Figure 5:A) The frequency distribution (the number of measurements that fell within an
570 interval of MFI) of γ -H2AX fluorescence for sham irradiated (0Gy) and irradiated cells
571 (0.05Gy and 0.5Gy). The black curve represents the probability density function and the
572 vertical black line represents the maximum probability of the probability density function. B)
573 The frequency distribution of the area of the region of the spectrum that was found to be
574 significantly higher following ionizing radiation. 27

575

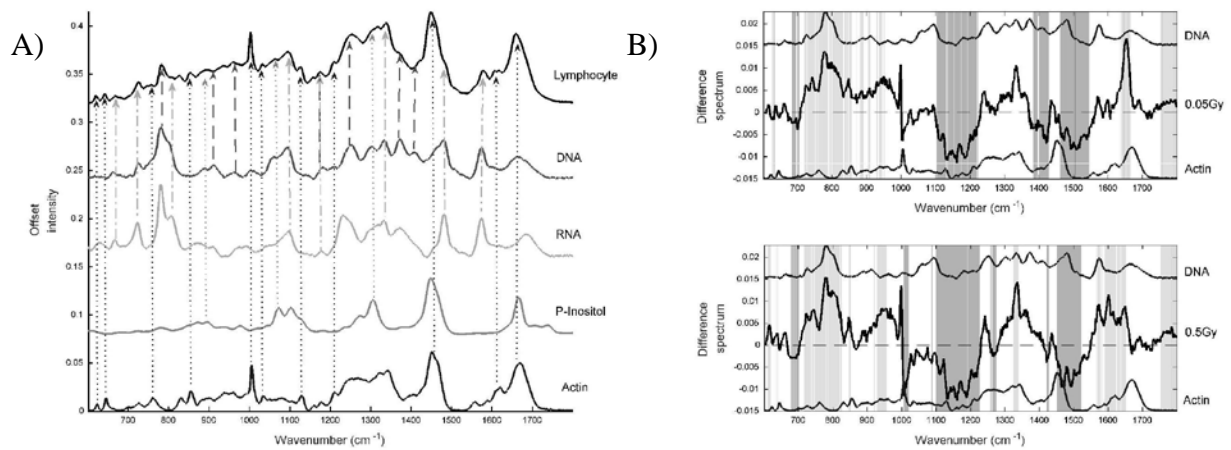
576 **10. List of tables**

577 Table 1: Raman band assignments for some typical vibrations associated with biological
578 specimens.....24

579 Table 2: Sensitivities and specificities for the classifications of 0Gy versus 0.05Gy, 0Gy
580 versus 0.5Gy and 0.05Gy versus 0.5Gy spectra for each donors spectra. Donors are ordered
581 in terms of decreasing sensitivities, larger sensitivities and specificities indicate larger
582 changes in spectral profiles following ionizing radiation.....28

583

584



586

587

588

589

590

591

592

593

594

Figure 1: A) The mean of all 20 donors sham-irradiated spectra along with spectra of DNA, RNA, phosphatidyl-inositol (a typical phospho-lipid) and actin (a typical protein). Guides are included to link some modes of vibration in component spectra to modes of vibration in lymphocytes. Pure DNA, RNA, phosphatidyl-inositol and actin were purchased from Sigma-Aldrich and used without further preparation.

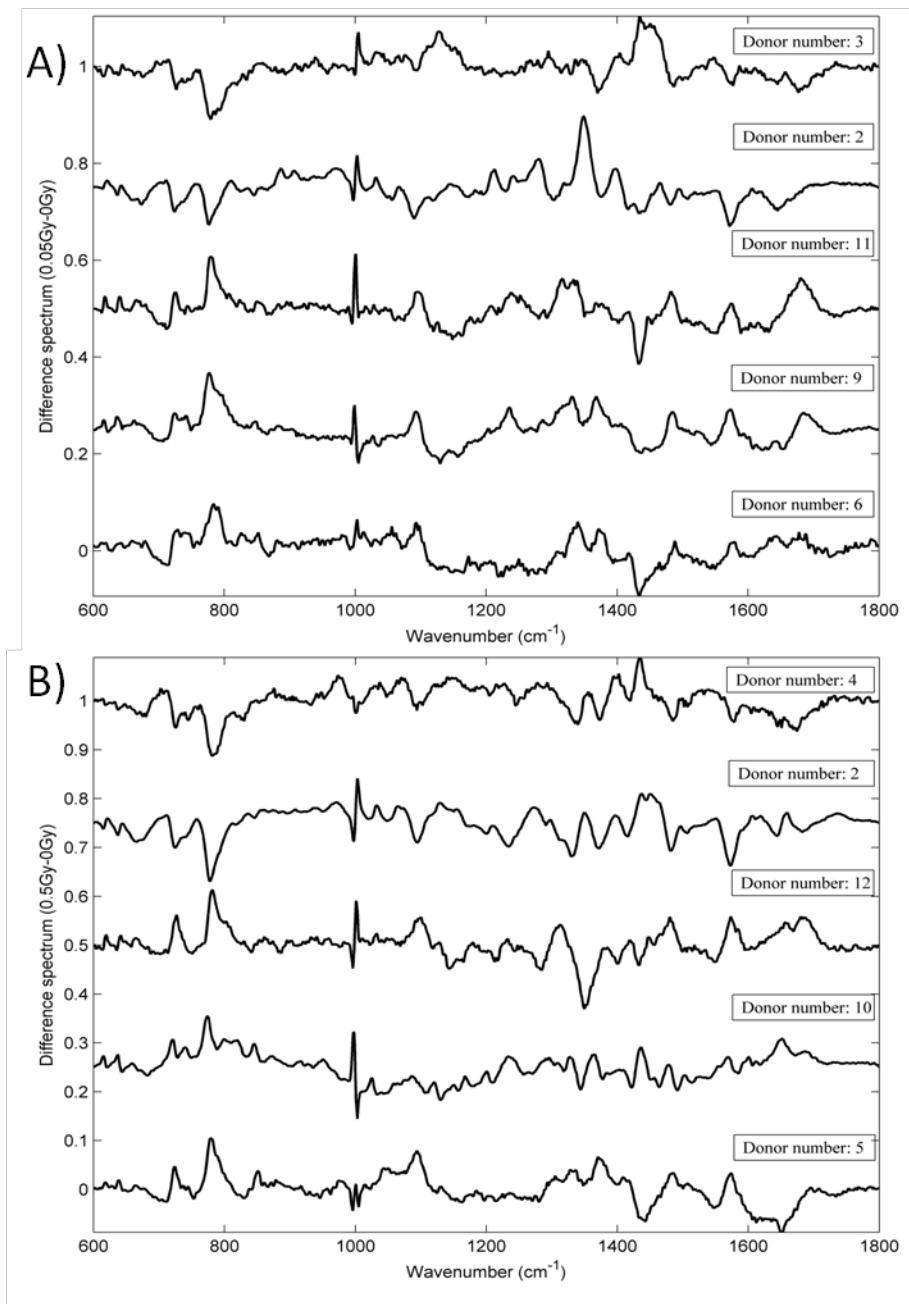
B) The difference spectra between sham irradiated and irradiated spectra (0.05Gy and 0.05Gy) along with spectra of DNA and actin. Shaded regions of the spectra represent where the spectrum of irradiated samples were found to be significantly higher (light shading) or significantly lower (darker shading) than the sham irradiated samples.

595 **Table 1:** Raman band assignments for some typical vibrations associated with biological specimens

596

Frequency (cm ⁻¹)	Assignment	Frequency (cm ⁻¹)	Assignment
623	C-C twisting mode phenylalanine.	1127	C-N, C-C stretching (protein and lipid)
645	Tyrosine		
666	Guanine, Thymine ring breathing	1175	Cytosine, Guanine, C-H bending
723	Adenine		tyrosine (proteins)
749	Tryptophan	1210	Tyrosine,
780	Cytosine, Uracil, Thymine (Ring breathing)	1230-1295	Phenylalanine
		1332	Amide III
807	O-P-O backbone (DNA/RNA)		C ₃ -C ₃ stretch, C ₅ -O ₅ stretch and CH _α in plane bending,
855	Tyrosine		Guanine
941	Skeletal modes (polysaccharides)	1370	Thymine, Adenine, Guanine
1003	Phenylalanine	1430-1460	C-H ₂ deformation
1032	C-H bending	1485	Amide II, Guanine, Adenine
1064	Phenylalanine ,C-C stretch of lipids	1552	Tryptophan
1085	C-O stretching	1575	Guanine, Adenine
1095	PO ₂ ⁻ from nucleic acids	1614/15	C=C (protein) Tyrosine, Tryptophan,
		1650-1680	Amide I, C=C stretching (proteins)

597



598

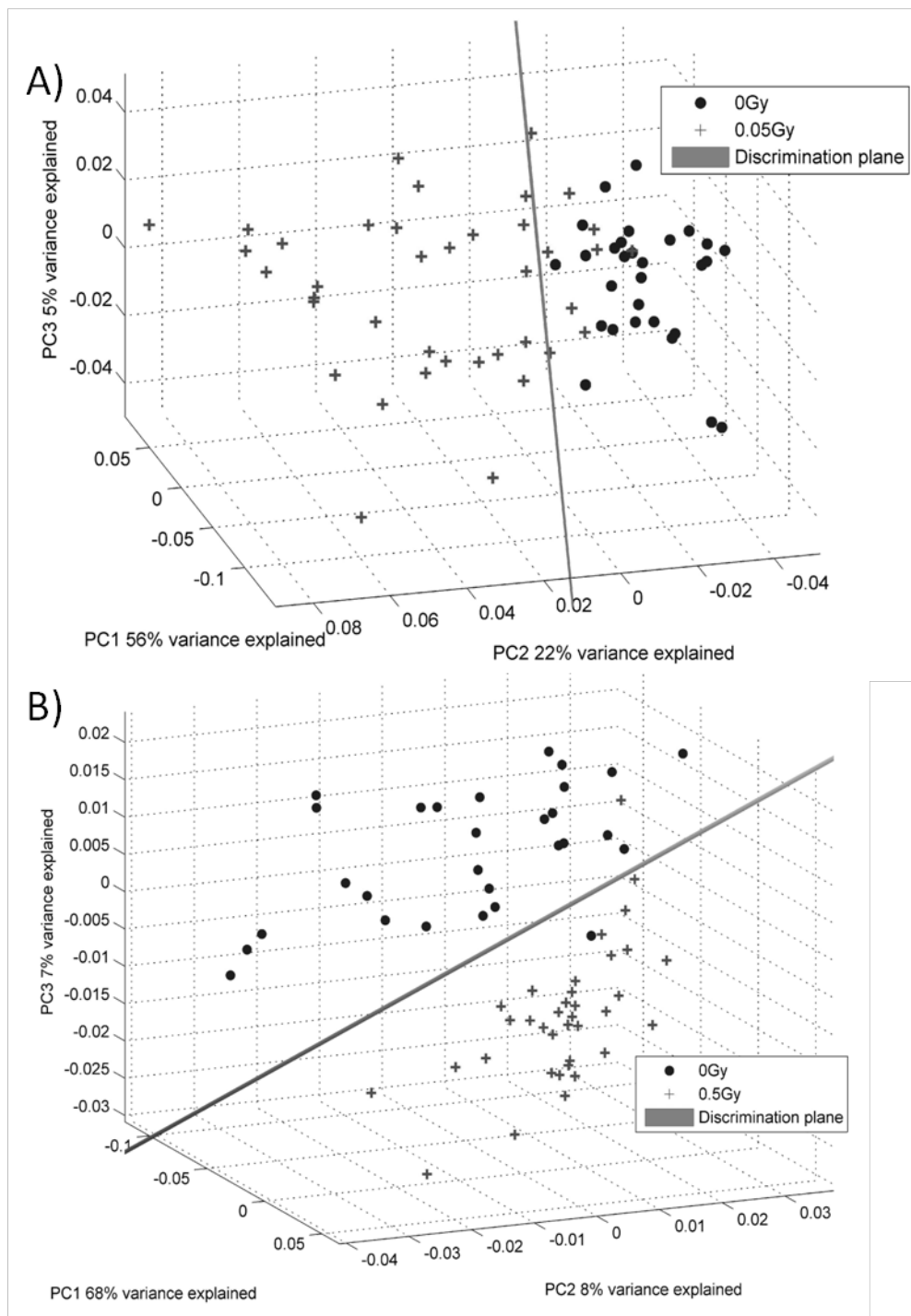
599

600

601

602

Figure 2: A) Difference spectra of 0.05Gy and 0Gy for 5 donor's spectra and B) Difference spectra of 0.5Gy and 0Gy for 5 donor's spectra.

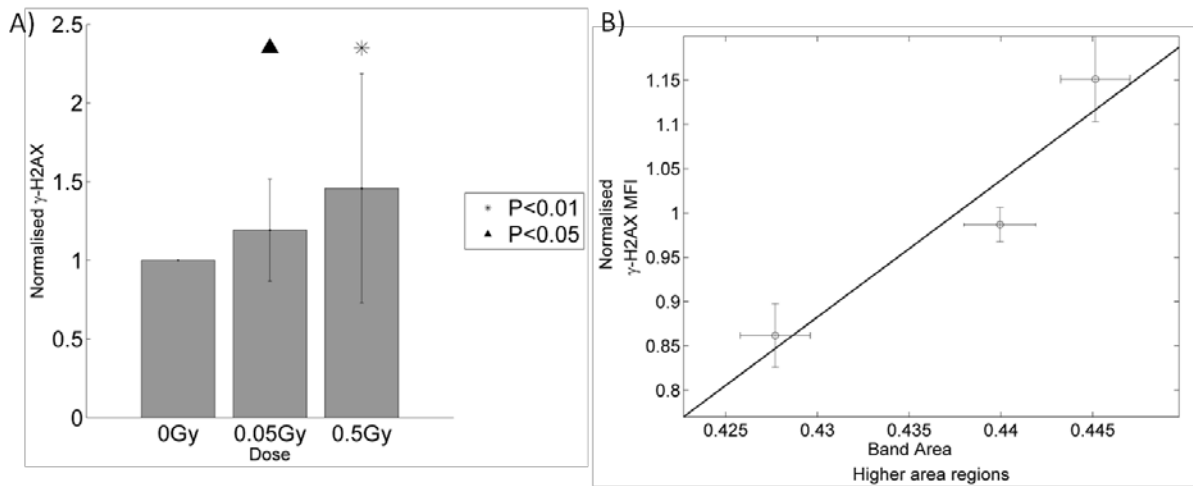


604

605

606

Figure 3: The scatter plots of PCA scores of 0Gy and 0.05Gy (A), and 0Gy and 0.5Gy (B) spectra of a single healthy donor and for the first three principal components. The grey line represents the plane of discrimination determined by LDA.



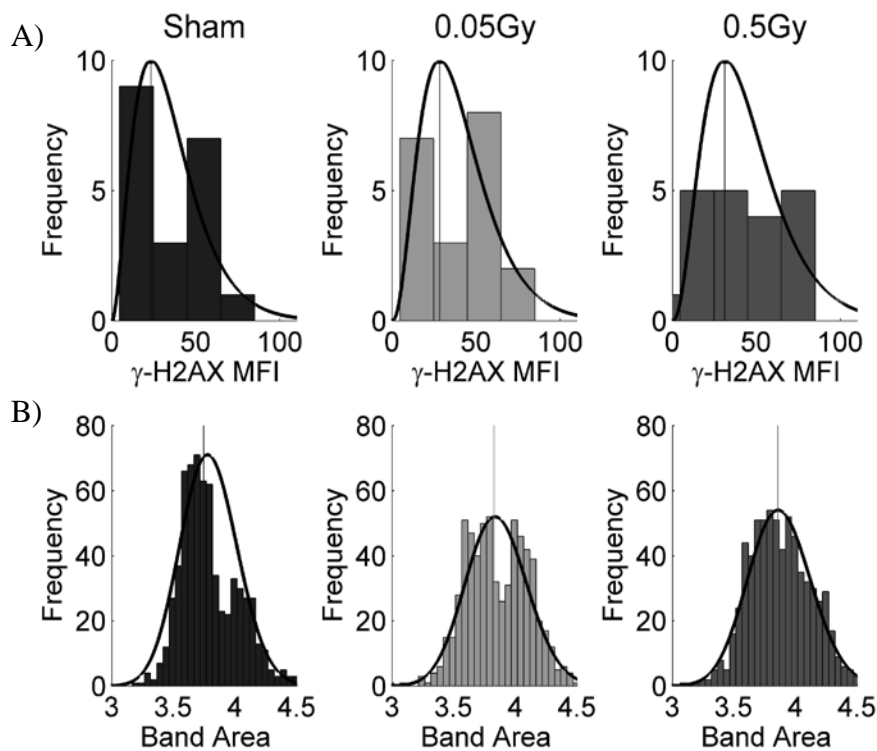
607

608

609

610

Figure 4: A) Normalised γ -H2AX fluorescence with respect to dose for all donors. Significance testing was performed using a two tailed paired t-test. B) Normalised γ -H2AX MFI with respect to the total area of the bands of the spectrum that were found to be significantly higher than the sham. Error bars indicate the standard error.



611

612

613

614

615

616

617

Figure 5: A) The frequency distribution (the number of measurements that fell within an interval of MFI) of γ -H2AX fluorescence for sham irradiated (0Gy) and irradiated cells (0.05Gy and 0.5Gy). The black curve represents the probability density function and the vertical black line represents the maximum probability of the probability density function. B) The frequency distribution of the area of the region of the spectrum that was found to be significantly higher following ionizing radiation.

618

619 **Table 2:** Sensitivities and specificities for the classifications of 0Gy versus 0.05Gy, 0Gy versus 0.5Gy and 0.05Gy versus

620 0.5Gy spectra for each donors spectra. Donors are ordered in terms of decreasing sensitivities, larger sensitivities and

621 specificities indicate larger changes in spectral profiles following ionizing radiation.

Donor no.	0.05Gy		Donor no.	0.5Gy		Donor no.	0.05Gy v 0.5Gy	
	Sensitivity	Specificity		Sensitivity	Specificity		Sensitivity	Specificity
10	1.00	1.00	2	1.00	1.00	1	1.00	1.00
11	1.00	0.96	8	1.00	1.00	2	1.00	1.00
15	1.00	0.94	10	1.00	1.00	15	1.00	1.00
9	0.97	0.92	20	1.00	1.00	7	1.00	1.00
2	0.96	1.00	1	1.00	0.97	8	1.00	1.00
8	0.95	0.94	15	1.00	0.90	5	1.00	0.93
20	0.93	1.00	12	0.98	0.96	19	1.00	0.88
7	0.93	0.86	19	0.97	0.92	12	0.97	0.94
19	0.92	0.94	5	0.97	0.97	13	0.97	0.97
18	0.91	0.91	7	0.96	0.86	10	0.97	0.90
14	0.91	1.00	14	0.93	1.00	17	0.97	0.82
3	0.90	0.93	3	0.92	1.00	20	0.96	0.91
12	0.90	0.85	9	0.92	0.89	16	0.91	1.00
1	0.86	0.84	17	0.91	0.83	9	0.90	0.97
13	0.82	0.94	16	0.86	0.97	6	0.90	0.82
5	0.81	1.00	6	0.86	0.93	18	0.88	1.00
6	0.79	0.89	18	0.84	0.91	3	0.85	0.93
4	0.76	0.80	4	0.82	0.91	14	0.82	0.92
16	0.71	0.82	13	0.81	0.89	11	0.81	0.73
17	0.67	0.82	11	0.78	0.85	4	0.79	0.79
Mean	0.90	0.92	Mean	0.93	0.94	Mean	0.94	0.93

622

623

624