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High sensitivity temperature sensor based on singlemode-no-core-singlemode fibre structure and alcohol

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1. Introduction

In recent years, singlemode-multimode-singlemode (SMS) fibre structures have attracted much research interest, primarily due to several advantages, including compact structure, ease of fabrication, and excellent compatibility with other photonic and optical fibre devices [1,2]. Relying on multimode interference (MMI) within the multimode waveguide and the resulting self-imaging phenomenon, SMS fibre structures have been widely applied in telecommunications, for example as wavelength division multiplexers [3], edge filters [4] and bandpass filters [5]. In addition, SMS fibre structures have also been successfully developed as optical fibre sensors for a wide variety of measurements, e.g. temperature [6], strain [7], curvature [8], humidity [9], refractive index (RI) [10] and magnetic fields [11,12]. SMS fibre structures can be easily adapted for a wide range of different applications due to the versatility of their fabrication and the fact that all versions (variants) rely on a common underlying operation principle i.e. MMI that exists within the multimode fibre (MMF).

Considerable research effort has been directed towards accurate temperature measurement over a long period as it is considered an im-

ABSTRACT

A high sensitivity temperature sensor based on a singlemode-no-core-singlemode (SNCS) fibre structure and surrounded with alcohol within a silica capillary is described. In this investigation, no-core fibre (NCF) is used as the multimode waveguide and alcohol is chosen as the temperature sensitive medium. By packaging the alcohol solution with a short length of NCF enclosed within a silica capillary, the surrounding temperature can be detected by monitoring the variations of transmission loss at a specific wavelength. The theoretical analysis predicts this temperature sensitivity of the sample is 0.49 dB/°C with a potential temperature resolution of 0.02 °C at the operating wavelength of 1545.9 nm. In addition, the repeatability and response time of the sensor of this investigation are investigated experimentally.

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portant physical parameter in many fields, and consequently, a wide variety of temperature sensors have been developed to date. When compared with traditional electronic temperature sensors e.g. thermocouples and thermistors, optical fibre based sensors exhibit a range of unique advantages including compact size, stability in hostile environments, inherent immunity to external electromagnetic interference, and excellent potential to offer high accuracy measurement (including high sensitivity) which is required for applications that involve to detecting very small temperature changes, for example in biological and medical diagnostics. Optical fibre temperature sensors have been predominantly based on fibre grating structures including fibre Bragg grating (FBG) [13] and long period grating (LPG) [14]. However, fibre grating structures generally offer a relatively low temperature sensitivity of circa 10 pm/°C. Various fibre interferometer based temperature sensors have become increasingly popular due to their excellent sensing performance, for example those based on the Mach-Zehnder interferometer (MZI) [15], the Fabry-Perot interferometer (FPI) [16], the Sagnac interferometer [17] and the Michelson interferometer [18]. However, in most cases, fibre interferometer based optical fibre sensors require a relatively complicated fabrication process which increases potential fabrication/manufacturing cost. In recent years, MMI based temperature sensors have attracted much research attention due to the advantages of potentially low raw material cost and ease of fabrication compared with other fibre optic sensing configurations. SMS fibre structures can be used in temperature measurement and this arises from the well-known thermo-optic and thermal expan-

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sion effects which are intrinsic material properties of silica optical fibre. Being dependent on this property, surrounding temperature changes produce a significant influence on MMI within MMF section, and monitoring the resulting spectral shift or intensity variation has been widely applied as an interrogation method in many reported temperature sensing scenarios [19–23]. However, SMS fibre structures based temperature sensors have often yielded relatively low intensity-temperature sensitivities (reported as optical transmission intensity per unit temperature) of about 0.0007 dB/°C [21], 0.0508 dB/°C [22] and 0.063 dB/°C [23], which can be attributed to the inherently low thermo-optic coefficients of the silica material. Thus, there is a clear need to develop a temperature sensor based on an SMS fibre structure that is easily fabricated, low-cost and which can offer higher measurement sensitivity.

In this paper, an optical fibre temperature sensor is described based on a singlemode-no-core-singlemode (SNCS) fibre structure surrounded by an alcohol layer. Alcohol was chosen as the temperature sensitive material to improve the sensing performance of the sensor due to its relatively high thermos-optic coefficient. The simulation analysis predicts this compact and simple structure can provide high sensitivity in terms of optical transmission intensity per unit temperature. The experiments undertaken as part of this investigation further support the existence of high sensitivity in this device. This indicates its potential applications in accurate bio-temperature monitoring as well as many other environment monitoring fields.

2. Principle and theoretical simulation

The schematic configuration of the proposed temperature sensor is shown in Fig. 1, an SNCS fibre structure is surrounded by alcohol solution within a silica capillary tube, and the two ends of the capillary tube were sealed using ultraviolet (UV) glue. In this investigation, the alcohol-immersed SNCS fibre structure is a generic SMS structure, in which the no-core fibre (NCF) is coupled between two optically aligned single-mode fibres (SMFs), and the NCF section and the surrounding sealed alcohol solution represent the multimode waveguide core and the associated cladding, respectively. It is well known that in an SMS fibre structure, the launched light from the input SMF can be assumed to be Gaussian with a radial field distribution of E(r,0)on account of the input SMF's circular symmetry and the fact that it supports transmission of only the fundamental mode. When the transmission light is launched into the NCF section, a series of high-order modes are excited and the input field can be decomposed into the eigenmodes of the linearly polarized (LP) mode of LPnm. However, in this case only the LP_{0m} modes can be effectively excited due to the circular symmetry of the input field and the assumption of ideal alignment between the SMF and NCF. For an alcohol-immersed NCF, the excited mode number M of the LP_{0m} can be calculated using:

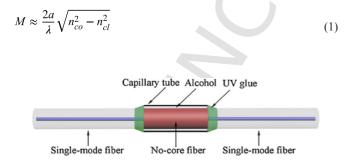


Fig. 1. Schematic of the sensing head based on an alcohol-immersed SNCS fibre structure.

where *a* is the radius of the NCF core, n_{co} and n_{cl} are the RI for the NCF core and the surrounding alcohol solution, respectively, and λ is the free space wavelength. By denoting the field profile of LP_{0m} as $\varphi_m(r)$, the input light field E(r, 0) of the NCF can be expressed as [24]:

$$E(r,0) = \sum_{m=1}^{M} c_m \varphi_m(r)$$
⁽²⁾

where *r* is radial distance in the cross section of the fibre, c_m is the excitation coefficient corresponding to the LP_{0m} mode, which can be calculated by the overlap integral between E(r, 0) and $\varphi_m(r)$ [25]:

$$c_m = \frac{\int_0^\infty E(r,0)\varphi_m(r)rdr}{\int_0^\infty \varphi_m(r)\varphi_m(r)rdr}$$
(3)

As the light propagates axially within the NCF section, the field at a propagation distance z can be calculated by [26]:

$$E(r,z) = \sum_{m=1}^{M} c_m \varphi_m(r) \exp(i\beta_m z)$$
(4)

where β_m is the propagation constant of each eigenmode of the NCF. MMI occurs within the NCF section between these excited high-order modes. When the light arrives at the output SMF, a portion of light from the NCF is coupled into the core of the output SMF, while the remaining light signal is coupled into the cladding and excites cladding modes which decay with a short distance. Ultimately, the resultant output optical intensity can be expressed as [12]:

$$I(\lambda) = \sum_{s=1}^{M} \eta_s^2 \cdot I_0(\lambda) + \sum_{s \neq m=1}^{M} \eta_s \cdot \eta_m \cdot I_0(\lambda) \cdot \cos(2\pi \Delta nL/\lambda)$$
(5)

where I_0 is the intensity of the LP₀₁ (fundamental mode) in the SMF, η_s and η_m is the coupling coefficient of the LP_{0s} and the LP_{0m} mode, respectively, Δn is the effective refractive index difference between the two modes and L is the length of the NCF. When the surrounding RI (outside the NCF) varies, the effective RIs of the different modes also changes, which influences the MMI and results in changes to the optical transmission intensity according to Eq. (5) above. Alcohol is chosen as the cladding material of the NCF because it is a widely available, can be easily infiltrated into the silica capillary of the device in this investigation and is a low-cost liquid but with a relatively high thermo-optic coefficient of -4×10^{-4} RIU/°C (a value confirmed in the experiments described below) which is two orders of magnitude higher than the equivalent value of 6.9×10^{-6} RIU/°C for silica fibre [27]. Utilizing the linear relationship between the RI of the alcohol solution and temperature, the external temperature can be measured based on an SNCS fibre structure combined with alcohol. It is worth noting that the temperature induced thermal expansion of the alcohol solution causes an extra stress in the silica capillary, however in practice this additional stress is so small that it can be ignored.

Based on the above theoretical analyses, numerical simulations have been conducted employing the beam propagation method (BPM) prior to fabrication of the sensor. The simulation conditions were based on a mesh size in the X, Y and Z directions of $0.1 \,\mu\text{m}$, 0.1 µm and 1 µm, respectively, and the boundary condition adopted a perfectly matched layer (PML) condition in the model. The length of NCF was chosen to be 4 cm which is an effective length to allow the occurrence of multimode interference (MMI) and this length is considered an optimal value to offer high temperature sensitivity [10,24]. The calculated optical field intensity distributions within the NCF section both before and after the injection of alcohol (the assumed RI value of the alcohol was 1.363 at 20 °C) at the wavelength of 1550 nm are presented in Figs. 2(a) and (b) respectively. The regular MMI pattern within the NCF section remains similar when the surrounding RI changes from 1 (the RI of air) to 1.363. The corresponding simulated transmission spectrum over the wavelength range of 1500 nm to 1600 nm is presented in Fig. 2(c). From Fig. 2(c), it is clear that the resonant wavelength evolves from dip₁ to dip₂ accompanied by a clear wavelength red shift (17.2 nm) and intensity decrease (3.58 dB) after alcohol is injected into the capillary tube.

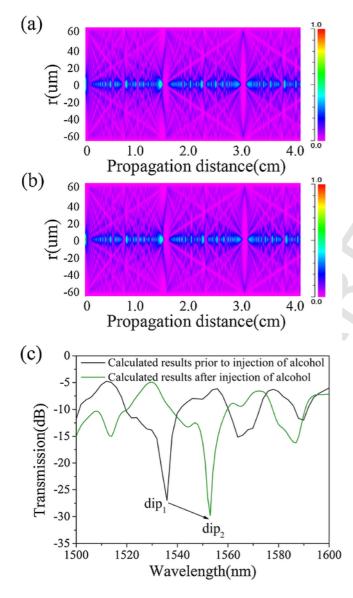


Fig. 2. Simulated optical field intensity distribution within an SNCS fibre structure (a) before injection of alcohol; (b) after injection of alcohol; (c) The corresponding transmission spectrum scanning from 1500 nm to 1600 nm.

To underpin a theoretical prediction for the amplitude change of the single wavelength dip₂ located at 1553 nm, it is necessary to know how the RI of the alcohol changes with temperature. For this purpose, the temperature dependence of the RI of the alcohol solution was experimentally measured and the results are shown in Fig. 3. It is clear that as the temperature increases, the RI of the alcohol solution exhibits a linear decrease (green line) with a slope value of temperature dependence circa -0.0004 RIU/°C which is consistent well with the result reported in [28]. Using this linear relationship, the amplitude of the 1553 nm dip was calculated at different temperatures. The calculated results (pink stars in Fig. 3) show that the intensity (in dB) of the 1553 nm dip is increased when the surrounding temperature increases from 20 °C to 45 °C. The data was fitted using a polynomial (quadratic) function which yielded a high correlation (fitting) coefficient of 0.9996. From the results, a maximum intensity-temperature sensitivity of 0.63 dB/°C was achieved at 20 °C. These simulation results predict that it is possible to fabricate a practical temperature sensor based on MMI employing an SNCS fibre structure and alcohol solution. Furthermore, it also demonstrates the feasibility of an interrogation scheme based on intensity changes at a single operating wavelength.

3. Experiments and discussion

The NCF used in this experiment was a commercially available product (Thorlabs FG125LA) which is made of pure silica with a diameter of 125 um, with an RI value of 1.444. A section of NCF with a length of 4 cm was initially stripped, cleaved, and optically connected between two single-mode fibres (SMF-28) using a standard fusion splicer (Fujikura 62S) to construct the SNCS fibre structure. The SNCS fibre structure was placed in the center of a capillary tube, whose inner diameter was 600 µm and length was 5 cm. Next, the alcohol solution was injected into the capillary tube with the help of capillary force. The concentration of the alcohol used in the experiment was 98%, and its RI was measured as 1.363 at 20 °C using an Abbe refractometer. Finally, to complete the fabrication process, the two ends of the capillary tube were sealed using UV curable glue to avoid alcohol leakage and evaporation. The measured transmission spectrum of the fabricated SNCS fibre structure is shown in Fig. 4 (blue line). The red line in Fig. 4 represents the transmission spectrum of the SNCS fibre structure after injection of alcohol. From Fig. 4, it can be observed that after the injection of alcohol, the interference

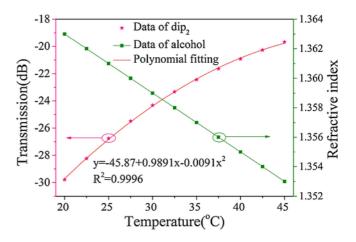


Fig. 3. Temperature dependence of refractive index of alcohol and simulated transmission loss (in dB) at single wavelength (1553 nm) when surrounding temperature changed.

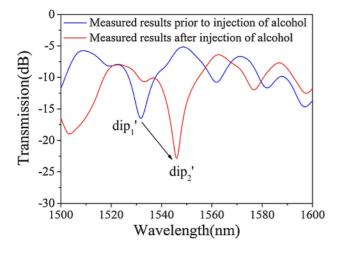


Fig. 4. Measured transmission spectra of the SNCS fibre structures before and after injection of alcohol.

dip₁' moved to a longer wavelength (a change of 14.1 nm). Also, the intensity of dip₁' exhibits a significant decline (increase in loss of 6.381 dB). The observed dip evolution is consistent with the simulated results presented in Fig. 2(c). The discrepancy that exists between the simulated and measured results can be attributed to the fact that the meridional axes of the SMF and NCF are not exactly in ideal central alignment [24]. Also there are some inherent approximations in the BPM simulation, for example only LP_{0m} modes were excited in the theoretical module. Furthermore, the solidification of the UV glue may also induce additional perturbation due to the microbend stress.

The experimental setup for temperature measurement using the proposed temperature sensor is schematically depicted in Fig. 5. The fabricated sample was placed on a temperature controlled thermoelectric Peltier cooler and fixed using UV glue to ensure that the sample can feed back surrounding temperature variation precisely and timely. A stable power supply (TTI EL302RT) was used to control the input electric current of the thermoelectric Peltier cooler, and the real-time temperature value on its surface was monitored using a thermocouple (RS 1313). The input SMF of the sample was connected to a broadband light source (BBS, Thorlabs S5FC1005S). The light was transmitted through the sensor and finally recorded by an optical spectrum analyzer (OSA, Agilent 86142B). The sample and the thermoelectric Peltier cooler were coved using a simple customized sealing (heat insulation) chamber to ensure more accurate temperature control in the experiments.

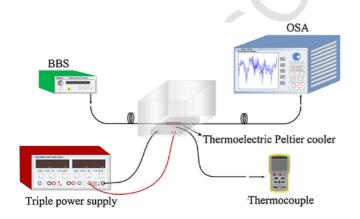


Fig. 5. Schematic diagram of the experimental setup for temperature measurement.

Fig. 6 shows the transmission spectrum evolution as the temperature was increased from 20 °C to 45 °C with an increment of 5 °C. From Fig. 6, it can be seen that the transmission loss (intensity) of the interference dip_2' (at the wavelength of 1545.9 nm) exhibits an expected increase (6.97 dB) as the temperature was increased from 20 °C to 45 °C. In addition, there is a small wavelength shift with the temperature increase, but this is not the focus of this investigation, as the sensor interrogation is planned to be purely intensity based. As in the case of the theoretical predictions, a clear relationship between temperature and transmission loss (in dB) is established. The dip transmission intensity was plotted (red marks) and fitted (red line) against temperature in the range of 20 °C to 45 °C in Fig. 7. The quadratic fitting curve exists a favorable relationship ($R^2 = 0.9942$) between the transmission intensity and temperature, and the maximum intensity-temperature sensitivity was 0.49 dB/°C when the temperature was 20 °C. Furthermore, given the limiting 0.3 dB intensity resolution of the OSA used in the experiments, the temperature resolution of the sensor system was calculated to be 0.61 °C. In practice the potential resolution achievable can be as good as 0.02 dB, for example replacing the detection device of OSA by a standard optical power meter with a higher intensity measurement resolution of 0.01 dB. Also a dedicated interrogation system with appropriate signal processing e.g. averaging should be applied to reduce the effect of noise.

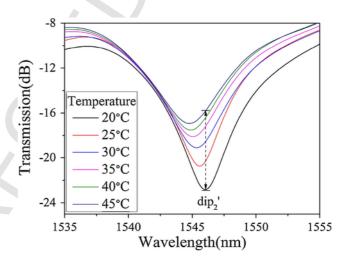


Fig. 6. Measured transmission spectrum evolution at varying temperature.

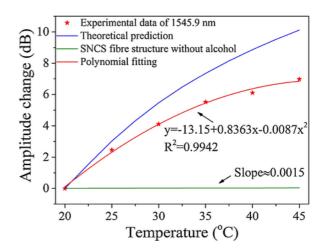
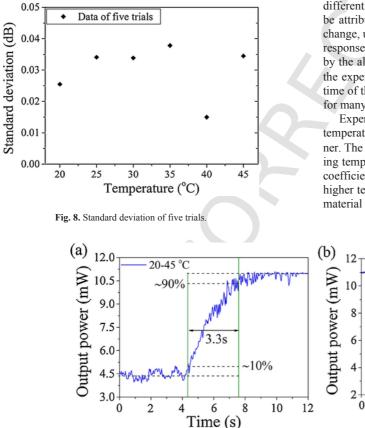


Fig. 7. Amplitude (transmission loss) changes as a function of temperature.

Fig. 7 also includes a direct comparison between the experimental and theoretical results. As shown in Fig. 7, there exists a good agreement between the measured results and the theoretical predictions, in that both fitting curves exhibit similar trends with temperature variation. The discrepancy between the measured and simulated results can be attributed to: (1) the thermo-optic and thermal expansion effects of optical fibre structure itself; (2) the extra stress applied to the structure due to thermal expansion effect of UV glue and alcohol; (3) some approximations in the simulation module as mentioned earlier in this section.

To further demonstrate the improved performance for temperature sensing due to the filled alcohol, a temperature sensing comparison experiment based on an SNCS fibre structure with the identical optical fibres but without surrounding alcohol was performed. The green line shown in Fig. 7 is the fitting result of the measured amplitude change (in dB) at a wavelength of 1531.8 nm (which is the central wavelength of dip₁' in Fig. 4) over the temperature range of 20 °C to 45 °C. From Fig. 7, it is clear that the achieved temperature sensitivity of SNCS fibre structure surrounded with alcohol is more than 300 times higher than that 0.0015 dB/°C of the SNCS fibre structure without alcohol, which is due to the high thermos-optic coefficient of alcohol. Based on the above results, a novel temperature sensor based on an SNCS fibre structure combined with alcohol by monitoring the amplitude (in dB) change at a single wavelength proved to be feasible.

In order to characterize the sensor more completely, the repeatability and response time of the proposed temperature sensor have also been investigated. To demonstrate the repeatability of the proposed fibre-optic temperature sensor, the sensor sample underwent



temperature cycling between 20 °C to 45 °C which was repeated five times. The standard deviation from the results of the five trials were calculated and the results are shown in Fig. 8. From the calculated results, the highest standard deviation is just 0.038 dB, which demonstrates the excellent repeatability of the sensor of this investigation. It is worth noting that the repeatability is significantly affected by the infiltration process of the alcohol solution. For example, if during the immersion process the amount of the alcohol solution injected is not sufficient to fill the space available, this can result in air bubbles within alcohol in the capillary tube which is found to reduce the repeatability. In addition, the UV glue must provide a good seal to prevent leakage and evaporation of the alcohol which can also impact negatively on the performance of the proposed sensor.

In the case of liquid-assisted temperature sensors, it is also important to determine response time. A tunable laser (NetTEST), a photo-detector and an oscilloscope (KEYSIGHT MSO-X 2022 A) were used to measure the response time of the sensor in this investigation. To examine the response time for increasing temperature, a step change in the temperature of the sensor structure is forced by abruptly attaching the sensor, previously at room temperature (20 °C), to the Peltier cooler with a set temperature of 45 °C. To examine the response to a decreasing temperature step, the sensor was abruptly removed from the Peltier cooler at 45 °C, in effect forcing a step decrease to the 20 °C room temperature environment. When the tunable wavelength was set at 1545.9 nm, the real-time output optical intensity variation was recorded using the oscilloscope. The 10% to 90% point method was used to calculate the response time [29]. Fig. 9(a) and (b) shows the calculated response times are 3.3 s and 5.4 s, respectively, when the temperature was increased from 20 °C to 45 °C and decreased from 45 °C to 20 °C. The measured response times are different in the case of temperature rise and drop scenarios. This can be attributed to the fact that an ideal and identical temperature step change, upward and downward are difficult to achieve in practice. The response time is limited by the thermal capacity of the sample formed by the alcohol's volume. Due to the small volume of alcohol used in the experiment (which was filled in the capillary tube), the response time of the proposed temperature sensor is within an acceptable range for many biomedical and environmental applications.

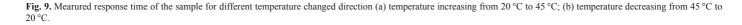
Experimental results have shown that this sensor can work over the temperature range of 20—45 °C in a highly stable and repeatable manner. The detectable temperature range is limited by the effective working temperature of the UV gel as well as the large thermal expansion coefficient of alcohol. Therefore, this sensor structure can access a higher temperature range if a more appropriate packaging and sealing material is adopted. In addition, whereas many optical fibre temperature

45-20 °C

90%

15 18 21 24

Time (s)



3 6 9 12

ture sensors' interrogation systems are based on wavelength shift, the temperature sensor in this investigation is based on intensity modulation. Thus, the OSA and the BBS which were used in the original experiment can be replaced by an optical power meter and a fixed wavelength LED or a laser light source with an appropriate choice of wavelength, which greatly reduces the overall cost of the measurement system.

4. Conclusion

A highly sensitive temperature sensor based on a singlemode-no-core-singlemode (SNCS) fibre structure in combination with alcohol has been described. In this investigation, no-core fibre (NCF) was used as the multimode waveguide and alcohol was chosen as the temperature sensitive medium acting effectively as a cladding. Through packaging alcohol with a short length of NCF within a sealed silica capillary, the surrounding temperature can be determined by monitoring the transmission loss at a specific wavelength. The experimental results show good agreement with the theoretical prediction, and a maximum temperature sensitivity of 0.49 dB/°C has been achieved experimentally with a potential temperature resolution of 0.02 °C at the operating wavelength of 1545.9 nm. Particularly, by monitoring the transmission loss change instead of wavelength shift, the cost of the temperature measurement system is significantly reduced. In addition, this temperature sensor has been demonstrated to have excellent repeatability and rapid response time, which confirms it can be potentially applied in different temperature monitoring scenarios including biomedical and environmental monitoring fields.

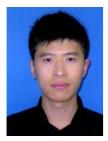
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